

论 著

基于IVIM-DWI多指数模型对卵巢肿瘤的良恶性鉴别及与ROMA指数的相关性分析*

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【摘要】目的 探讨基于体素内不相干运动扩散加权成像(IVIM-DWI)的多指数模型对卵巢肿瘤的良恶性鉴别及与卵巢恶性肿瘤风险算法(ROMA)指数相关性分析。方法 共收集卵巢良性肿瘤39例与恶性肿瘤30例,临床和影像学资料均完整。基于IVIM-DWI多指数模型参数比较卵巢良恶性肿瘤的组间差异及各参数效能分析;再对上皮性卵巢癌(22例)IVIM-DWI各参数值与ROMA指数进行Spearman相关性分析。结果 卵巢良恶性肿瘤的IVIM-DWI多指数模型各定量参数组间比较差异显著,结果均有统计学意义($P<0.05$);其中Dslow、ADCstand及f对卵巢良恶性肿瘤的鉴别具有较高的诊断效能敏感性分别为86.67%,90%,72.33%,特异性分别为82.05%,87.18%,92.31%;上皮性卵巢癌ADCstand及Dslow值与ROMA指数呈负相关。结论 IVIM-DWI多指数模型联合ROMA指数有助于卵巢肿瘤的良恶性鉴别,可作为评估上皮性卵巢癌的有效生物学指标。

【关键词】卵巢肿瘤;体素内不相干运动;扩散加权成像;卵巢恶性肿瘤风险算法(ROMA);鉴别诊断

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Differentiation of Benign and Malignant Ovarian Tumors Based on IVIM-DWI Multi-Exponential Model and Correlation Analysis with ROMA Index*

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ABSTRACT

Objective To investigate the multi-exponential model based on intra-voxel incoherent motion diffusion-weighted imaging for the differentiation of benign and malignant ovarian tumors and the correlation analysis with the risk algorithm index of ovarian malignancy. **Methods** A total of 39 cases of benign ovarian tumors and 30 cases of malignant tumors were collected, and the clinical and imaging data were complete. Based on the IVIM-DWI multi-exponential model parameters, the differences between groups of ovarian benign and malignant tumors and the performance analysis of each parameter were compared. Then, the Spearman correlation analysis was performed on the IVIM-DWI parameters of epithelial ovarian cancer and the ROMA index. **Results** The quantitative parameters of IVIM-DWI multi-exponential model of ovarian benign and malignant tumors were significantly different between groups, and the results were all statistically significant ($P<0.05$). The efficacy sensitivity was 86.67%, 90%, 72.33%, and the specificity was 82.05%, 87.18%, 92.31%, respectively. The ADCstand and Dslow values of epithelial ovarian cancer were negatively correlated with the ROMA index. **Conclusion** IVIM-DWI multi-exponential model combined with ROMA index can help differentiate benign and malignant ovarian tumors, and can be used as an effective biological indicator for evaluating epithelial ovarian cancer.

Keywords: Risk of Ovarian Malignancy Algorithm; Ovarian Tumor; Incoherent Motion Voxel; Diffusion Weighted Imaging; Differential Diagnosis

卵巢癌居妇科恶性肿瘤第三位,但是由于其早期症状缺乏特异性且病灶隐匿,因此卵巢癌的总预后较差且预后与诊断分期密切相关^[1-2],因此早期发现有助于提高生存率。以往的研究发现基于单一b值算法的磁共振扩散加权成像(diffusion weighted imaging, DWI)对卵巢肿瘤的良恶性鉴别以及指导手术计划方面起着至关重要的作用^[3-4],但是单b值参数易受组织灌注影响。近年来,通过多b值DWI进行体素内不相干运动(intravoxel incoherent motion, IVIM)的非高斯扩散模型得到广泛关注,能够反映活体组织内的水分子扩散与微循环灌注情况。其中,双指数模型将体内不规则运动区分为灌注相关的快速扩散和水分子运动的缓慢扩散状态^[5];但拉伸指数模型是一种新拟合的能够体现表观扩散衰减特征的算法,主要反映标准扩散系数在体素内的连续分布状态,可对体内异质性进行量化^[6]。但基于IVIM多指数扩散模型的卵巢肿瘤研究尚不多见。此外,卵巢恶性肿瘤风险算法(risk of ovarian malignancy algorithm, ROMA)是基于人附睾蛋白4和糖类抗原125及更年期状态对女性盆腔肿块恶性风险进行分类评分的指数模型,临床试验中其总体敏感性达93.8%,特异性为74.9%^[7-8]。本研究旨在通过分析基于IVIM的单指数模型并与ROMA指数进行相关性分析,评估基于IVIM-DWI多指数模型对卵巢良恶性肿瘤鉴别诊断的应用价值。

1 资料与方法

1.1 临床资料 收集我院2019年6月至2021年5月临床资料完整并且经手术病理证实的卵巢肿瘤共69例(1例乳腺癌合并卵巢转移瘤系经临床及影像检查明确诊断),患者术前均行盆腔MR常规+多b值DWI+增强检查。临床症状主要包括腹痛、腹胀、腹部触及肿块或月经不规律等。所有患者行盆腔MRI检查前卵巢肿块未接受过相关任何治疗。

排除标准:卵巢生理性囊肿、囊性畸胎瘤或子宫内膜异位症;怀孕;DWI图像质量较差(如节育环伪影),影响测量结果。本研究通过了常熟市第二人民医院伦理委员会的批准(2016023)并同意免除患者知情同意权。

1.2 检查方法 磁共振成像系统采用3.0T MR GE Discovery 750M扫描仪(GE healthcare, USA)和16通道腹部相控阵线圈(GE Health care)。检查前需禁食4~6h。多b值DWI扫描采用轴位单次激发平面回波成像(EPI)序列,TR 2600.00 ms, TE 71.50 ms,层厚/层间距为5.0 mm/1.0 mm,矩阵160×160,FOV 340.0 mm×340.0 mm,

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并行采集因子2;共设定11个b值,分别为0、30、50、100、150、200、400、600、800、1000、1500s/mm²,b值为0、600s/mm²时激励次数为2,b值为30-400s/mm²时激励次数为1,b值为800、1000、1500s/mm²时激励次数分别为3、4、5。常规扫描包括轴位快速自旋回波序列T₁WI(TR 700ms,TE 7ms),层厚/层间距为5.0 mm/1mm;横轴面、矢状位和冠状位快速恢复快速自旋回波序列T₂WI:TR(7000ms,TE 100ms),层厚/层间距为4.0mm/0.4mm。增强扫描采用肝脏速容积采集序列轴面、矢状面及冠状面扫描(TR 3.05ms,TE 1.44ms),对比剂使用钆喷替酸葡甲胺(Gd-DTPA),高压注射器静脉推注,0.2mL/kg;层厚/层间距为4mm/0mm。

1.3 图像分析及数据测量 利用工作站自带软件GE Functool MADC对DWI图像原始数据进行多参数后处理分析。由2名主治医师及以上的放射科医师共同商定完成数据测量。以T₂WI图像作为参照,考虑到在b值为1000s/mm²时图像的T₂效应干扰较小且信噪比较高,故选择此b值的DWI轴位图像上进行各参数的定量测定。感兴趣区(region of Interest, ROI)的确定遵循原则为:(1)经两位放射科医生一致讨论形态学特征的识别和感兴趣区域ROI位置的选择,在常规T₁和T₂加权图像肿瘤最大层面上确定形态学特征(最大直径、实性成分等);(2)将ROI置于病灶实性区域或分隔处,避开囊变、坏死区;(3)放置不同部位测量3次取平均值,ROI面积≥50mm²。测量参数包括:(1)单指数模型参数:标准扩散系数(standard apparent diffusion coefficient, ADCstand),ADCstand采用两个b值(0, 1000s/mm²)的标准单指数模型计算^[3],近似于传统单b值ADC;(2)双指数模型参数:纯扩散系数(true-apparent diffusion coefficient,Dslow)、快速表现扩散系数(pseudo-apparent diffusion coefficient,Dfast)及灌注分数(perfusion fraction,f)^[5];(3)拉伸指数模型参数:分布扩散系数(distributed diffusion coefficient, DDC)及拉伸因子(stretched exponential,α),α从0到1变化,表示信号衰减与单指数衰减的偏差^[6]。

1.4 ROMA指数检测及判定标准 ROMA预测指数依据受试者的人附睾蛋白4、糖类抗原125检测值和绝经状况进行公式推算^[8]。检测分析仪采用雅培诊断产品有限公司(上海)。根据雅培实验室

诊断,绝经前患者检测数值≥7.4%定为阳性;绝经后患者检测数值≥25.3%定为阳性;其他情况定为阴性^[9]。

1.5 统计学分析 统计学分析使用SPSS(版本23.0)及Medcalc(版本19.0.4)软件进行统计学分析。首先使用shapiro-wilk检验方法对两组受试者的临床计量资料、ROMA指数及IVIM-DWI各参数测量值行正态分布检验,计量资料符合正态分布时用均数±标准差($\bar{x} \pm s$)表示,非正态分布时用中位数(四分位数)表示,并采用独立样本t检验或曼-惠特尼U检验比较卵巢恶性肿瘤的组间差异。计数资料比较采用 χ^2 检验。采用受试者工作特征(receiver operating characteristic, ROC)曲线评价IVIM-DWI多指数模型各参数值鉴别良恶性肿瘤的曲线下面积(Area Under Curve, AUC)、诊断阈值、敏感性及特异性;采用Spearman非等级资料相关性分析各参数值和上皮性卵巢癌ROMA指数的相关性。 $P < 0.05$ (双尾)为差异有统计学意义。

2 结果

2.1 病理结果 共收集卵巢肿瘤69例,其中卵巢良性肿瘤共39例(上皮细胞性肿瘤29例,性索间质肿瘤7例,卵巢二元碰撞瘤2例,生殖细胞肿瘤1例),年龄18~84岁;卵巢恶性肿瘤共30例(上皮性卵巢癌22例,恶性性索间质源性肿瘤1例,恶性生殖细胞肿瘤1例,转移性肿瘤6例),年龄31~81岁。两组间年龄及ROMA指数比较均有统计学差异,绝经状态无统计学差异,具体见表1。

2.2 卵巢良恶性肿瘤IVIM-DWI多指数模型定量参数测量结果比较以及诊断效能 卵巢良恶性肿瘤IVIM-DWI多指数模型定量参数测量结果显示两组间各参数值比较均存在显著性差异($P < 0.05$),其中良性肿瘤组的ADCstand、Dslow、Dfast、DDC及α值均高于恶性肿瘤组,f值低于恶性肿瘤组,具体见表2。对卵巢良恶性肿瘤鉴别诊断效能最高的参数为Dslow,其次是ADCatand及f,AUC值分别为0.94、0.90、0.90,具体见表3(图1~图2)。

2.3 Spearman相关性分析 IVIM-DWI多指数模型各参数与上皮性卵巢癌(n=22)ROMA指数的Spearman相关性分析显示上皮性卵巢癌ADCstand及Dslow值与ROMA指数呈负相关($r = -0.465$, $P = 0.029$; $r = -0.543$, $P = 0.009$)(图3),而Dfast、f、DDC及α值与ROMA指数均无相关性。

表1 卵巢良恶性肿瘤临床资料组间比较

病例(n)	年龄	绝经状态(n)	ROMA指数
良性肿瘤组			
浆液性囊腺瘤(17/39)	50.51±17.12	绝经前(14/39)	10.09±5.15
粘液性囊腺瘤(10/39)		绝经后(25/39)	
Brenner瘤(2/39)			
卵泡膜纤维瘤(7/39)			
浆液性囊腺瘤伴卵泡膜纤维瘤(2/39)			
畸胎瘤(1/39)			
恶性肿瘤组			
高级别上皮性卵巢腺癌(15/30)	57.90±11.96	绝经前(8/30)	63.39±36.94
交界性上皮性肿瘤(4/30)		绝经后(22/30)	
低级别上皮性卵巢囊腺癌(3/30)			
颗粒细胞瘤(1/30)			
恶性畸胎瘤(1/30)			
转移性肿瘤(6/30)			
t/ χ^2 值	2.11	0.58	7.70
P值	0.039	0.317	<0.001

表2 卵巢良恶性肿瘤IVIM-DWI多指数模型参数测量组间结果比较[中位数(四分位数)]

参数	良性肿瘤组	恶性肿瘤组	Z值	P值
ADCstand($\times 10^{-3}$ mm ² /s)	2.30(1.66,2.61)	0.90(0.74,1.32)	5.71	<0.001
Dslow($\times 10^{-3}$ mm ² /s)	2.18(1.55,2.73)	0.81(0.72,1.15)	5.13	<0.001
Dfast($\times 10^{-3}$ mm ² /s)	20.33(10.34,26.11)	2.87(1.58,6.42)	5.88	<0.001
f	0.21(0.05,0.43)	0.70(0.49,0.80)	5.71	<0.001
DDC	1.61(1.05,1.96)	0.76(0.58,0.98)	4.79	<0.001
α	0.77(0.71,0.86)	0.70(0.63,0.79)	3.07	0.003

表3 IVIM-DWI多参数对卵巢良恶性肿瘤的鉴别诊断效能分析

参数	AUC	诊断阈值	敏感度(%)	特异度(%)	95%可信区间
ADCstand	0.90	1.49	86.67	82.05	(0.81, 0.96)
Dslow	0.94	1.47	90.00	87.18	(0.85, 0.98)
Dfast	0.79	14.41	86.67	64.10	(0.79, 0.95)
f	0.90	0.52	72.33	92.31	(0.81, 0.96)
DDC	0.84	0.84	70.00	89.74	(0.73, 0.92)
α	0.69	0.72	71.80	60.00	(0.57, 0.82)

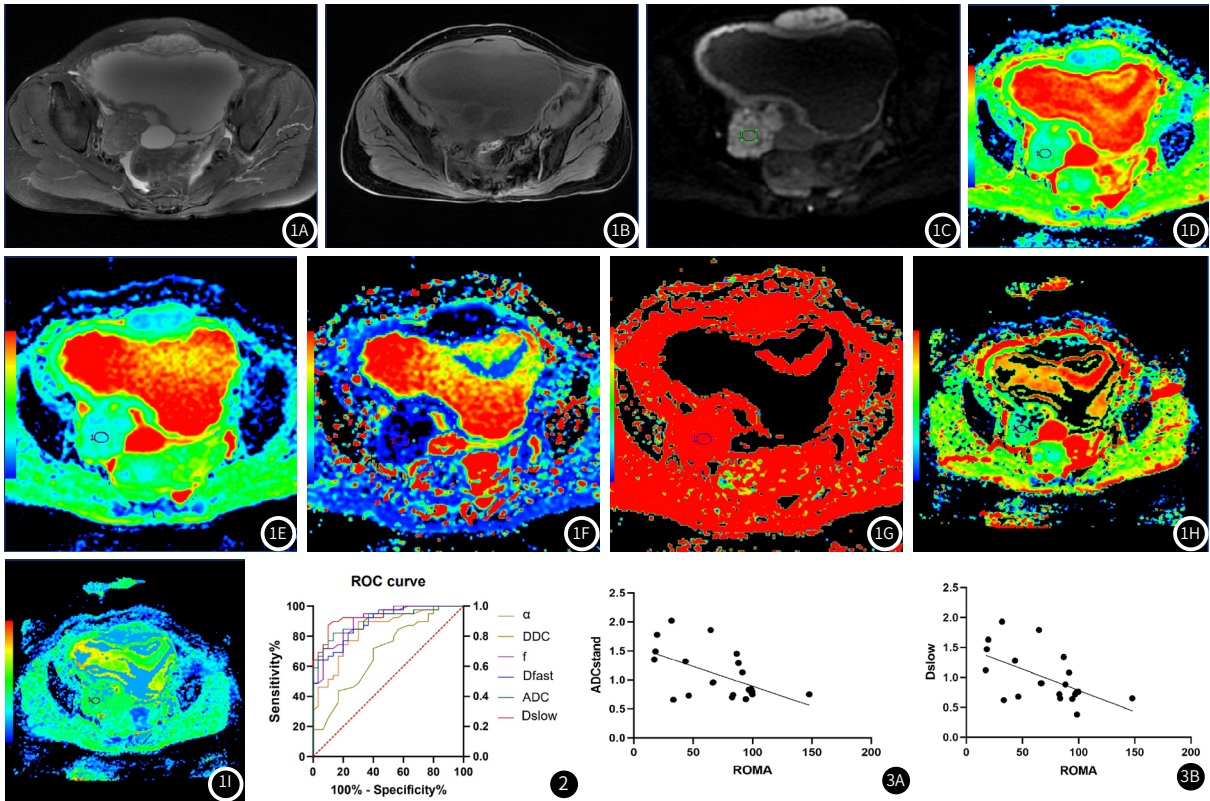


图1 女, 53岁, 右侧卵巢高级别浆液性囊腺癌。图1A~图1B分别为盆腔常规平扫T₁WI、T₂WI图像, 盆腔内可见较大囊实性肿块; 图1C为高b值DWI图像(b值=1000s/m²), 肿块的实性部分呈明显高信号, 并ROI放置于肿块实性区域; 图1D~图1I分别为ROI获得ADCstand、Dslow、Dfast、f、DDC及 α 测量值的伪彩图。图2 IVIM-DWI多参数对卵巢良恶性肿瘤的鉴别诊断效能ROC曲线图。其中参数Dslow、ADCstand和f对卵巢良恶性肿瘤的鉴别诊断效能较高, 敏感性分别为86.67%, 90%, 72.33%, 特异性分别为82.05%, 87.18%, 92.31%。图3 图3A~图3B分别为上皮性卵巢癌ADCstand及Dslow与ROMA指数的Spearman相关性分析。

3 讨论

针对IVIM-DWI单指数模型及双指数模型参数, 我们的研究结果表明卵巢恶性肿瘤的ADCstand、Dslow、Dfast值明显低于良性肿瘤, f值高于良性肿瘤。由于卵巢恶性肿瘤细胞密度的增加和细胞外空间的减少, 导致水分子的扩散更加受阻, 故ADCstand和Dslow值减小。在低b值(<200s/mm²)时, 微循环灌注对MR信号衰减影响的较大^[10], 而IVIM双指数模型Dslow值是经高b值拟合得出, 故避免了微循环灌注的影响, 同时反映了组织的纯扩散信息。本研究中卵巢良性肿瘤及恶性肿瘤各组内的ADCstand值均大于Dslow值, 说明参数Dslow能够通过消除灌注的影响来维持真正的扩散。此外参数Dslow、ADCstand和f在区分卵巢良恶性肿瘤时具有较高的AUC值(分别为0.94、0.90和0.90), 其中Dslow的敏感性和特异性均较高(90%, 87.18%), 这也表明Dslow在区分卵巢良恶性肿瘤方面可能比ADCstand更精确。

参数Dfast主要反映血流量状态, 与微血管密度和微血管内血流速度密切相关^[11]。Dfast值低表明血流灌注水平低, 反映了肿瘤细胞的血供相对较弱。本研究中卵巢恶性肿瘤组Dfast值较良性肿瘤组低, 原因可能是卵巢恶性肿瘤细胞增殖较快, 肿瘤血管生成因子过度表达同时新生血管功能和结构异常, 致使具有灌注功

能的血管比例下降^[12]。但以往部分研究结果^[13]显示两组间Dfast无统计学差异。相互矛盾的结果可能与不同的b值、信号强度比和肿瘤组织学异质性不同导致Dfast诊断特异性及重复性较低有关^[11,14]。合适的低b值数量设定对于捕捉IVIM成像的初始快速衰减至关重要, 因为设定的低b值参数数量较少时Dfast值往往被低估, 而数量较多时又会被高估^[15,16]。此外, 参数f反映微血管血流在体素水平上的体积分数^[17], 即每单位肿瘤体积中, 良性肿瘤的毛细血管数量相对较少, 而恶性肿瘤的毛细血管数量较多。本研究中, 卵巢恶性肿瘤组的f值显著高于良性肿瘤组, 说明与卵巢恶性肿瘤的组织血管密度与良性肿瘤相比较, 参数f在无创性评估卵巢恶性肿瘤血管生成活性方面具有较大的潜力。

针对IVIM拉伸指数模型参数, 我们的研究结果表明卵巢恶性肿瘤的DDC值及 α 值均低于良性肿瘤组。DDC被认为是ADC连续分布的加权和, 代表多指数衰减, 可综合反映肿瘤内水分子扩散状态^[18]。本研究中的ROC曲线表明参数DDC的特异性较ADCstand高, 但敏感性稍低。参数 α 主要反映肿瘤的异质性, 包括细胞高度异型现象、肿瘤新生的微血管和血管结构的异质性等^[19], 本研究中卵巢良性肿瘤的 α 值比恶性肿瘤高, 意味着后者的组织扩散异质性较好, 而肿瘤内异质性对临床结果和治疗反应的

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参考文献

[1] Zethraeus N, Borgström F, Ström O, et al. Cost-effectiveness of the treatment and prevention of osteoporosis—a review of the literature and a reference model[J]. *Osteoporos Int*, 2007, 18(1): 9–23.

[2] Borgström F, Sobocki P, Ström O, et al. The societal burden of osteoporosis in Sweden[J]. *Bone*, 2007, 40(6): 1602–1609.

[3] Jarvinen SR, Yuan HA, Reiley MA, et al. New technologies in spine: kyphoplasty and vertebroplasty for the treatment of painful osteoporotic compression fractures[J]. *Spine (Phila Pa 1976)*, 2001, 26(14): 1511–1515.

[4] Venmans A, Klazen CA, Lohle PN, et al. Percutaneous vertebroplasty and pulmonary cement embolism: results from VERTOS II[J]. *AJNR Am J Neuroradiol*, 2010, 31(8): 1451–1453.

[5] Al-Nakshabandi NA. Percutaneous vertebroplasty complications[J]. *Ann Saudi Med*, 2011, 31(3): 294–297.

[6] 袁德超, 吴超, 邓佳燕, 等. 基于Mimics软件分析椎体成形术后骨水泥形态和弥散程度的临床意义[J]. *中国组织工程研究*, 2019, 23(10): 1507–1513.

[7] Lamy O, Uebelhart B, Aubry-Rozier B, et al. Risks and benefits of percutaneous vertebroplasty or kyphoplasty in the management of osteoporotic vertebral fractures[J]. *Osteoporosis international*, 2014, 25(3): 807–819.

[8] Bae JS, Park JH, Kim KJ, et al. Analysis of Risk Factors for Secondary New Vertebral Compression Fracture Following Percutaneous Vertebroplasty in Patients with Osteoporosis[J]. *World Neurosurg*, 2017, 99: 387–394.

[9] Sun YC, Teng MM, Yuan WS, et al. Risk of post-vertebroplasty fracture in adjacent vertebral bodies appears correlated with the morphologic extent of bone cement[J]. *J Chin Med Assoc*, 2011, 74(8): 357–362.

[10] 侯文根, 孙晓辉, 张超, 等. 老年椎体压缩性骨折患者经皮椎体成形术后邻近椎体骨折的发生率及相关危险因素分析[J]. *中国矫形外科杂志*, 2016, 24(20): 1909–1911.

[11] Baek SW, Kim C, Chang H. The relationship between the spinopelvic balance and the incidence of adjacent vertebral fractures following percutaneous vertebroplasty[J]. *Osteoporos Int*, 2015, 26(5): 1507–1513.

[12] Han SL, Wan SL, Li QT, et al. Is vertebroplasty a risk factor for subsequent vertebral fracture, meta-analysis of published evidence?[J]. *Osteoporos Int*, 2015, 26(1): 113–122.

[13] Voormolen MH, Lohle PN, Juttman JR, et al. The risk of new osteoporotic vertebral compression fractures in the year after percutaneous vertebroplasty[J]. *J Vasc Interv Radiol*, 2006, 17(1): 71–76.

[14] Uppin AA, Hirsch JA, Centenera LV, et al. Occurrence of new vertebral body fracture after percutaneous vertebroplasty in patients with osteoporosis[J]. *Radiology*, 2003, 226(1): 119–124.

[15] Li YA, Lin CL, Chang MC, et al. Subsequent vertebral fracture after vertebroplasty: incidence and analysis of risk factors[J]. *Spine (Phila Pa 1976)*, 2012, 37(3): 179–183.

[16] McKiernan F, Faciszewski T. Intravertebral clefts in osteoporotic vertebral compression fractures[J]. *Arthritis Rheum*, 2003, 48(5): 1414–9.

[17] Yu W, Jiang X, Liang, et al. Intravertebral Vacuum Cleft and Its Varied Locations within Osteoporotic Vertebral Compression Fractures: Effect on Therapeutic Efficacy[J]. *Pain Physician*, 2017, 20(6): E979–E986.

[18] Wei P, Yao Q, Xu Y, et al. Percutaneous kyphoplasty assisted with/without mixed reality technology in treatment of OVCF with IVC: a prospective study[J]. *J Orthop Surg Res*, 2019, 14(1): 255.

[19] Rohlmann A, Boustani HN, Bergmann G, et al. A probabilistic finite element analysis of the stresses in the augmented vertebral body after vertebroplasty[J]. *Eur Spine J*, 2010, 19(9): 1585–1595.

[20] Khosla A, Diehn FE, Rad AE, et al. Neither subendplate cement deposition nor cement leakage into the disk space during vertebroplasty significantly affects patient outcomes[J]. *Radiology*, 2012, 264(1): 180–186.

[21] 蔡金辉, 刘庆余, 曾玉蓉, 等. MRI预测经皮椎体强化术骨水泥椎间盘渗漏的价值[J]. *中国医学影像技术*, 2017, 33(7): 1061–1065.

[22] 张晓星, 代灿, 邓志龙, 等. 不同手术方法治疗骨质疏松性椎体压缩性骨折[J]. *中国中西医结合外科杂志*, 2019, 25(1): 22–26.

[23] Kim HS, Ju CI. Spinal Instability Predictive Scoring System for Subsequent Fracture After Bone Cement Augmentation in Patients with Osteoporotic Vertebral Compression Fracture[J]. *World Neurosurg*, 2017, 106: 736–745.

[24] Layton KF, Thielen KR, Koch CA, et al. Vertebroplasty, first 1000 levels of a single center: evaluation of the outcomes and complications[J]. *AJNR Am J Neuroradiol*, 2007, 28(4): 683–689.

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影响较大^[20]; 但是 α 的特异性稍低(60%), 原因可能是进行ROI测量时选择病变的实体区域而不是整个病变, 可能会由于组织病理学的异质性而导致一些选择偏差。

参数ADCstand与Dslow与上皮性卵巢癌ROMA指数呈负相关, 这表明二者可作为评估上皮性卵巢癌的生物标记物。ROMA指数与上皮性卵巢癌的级别密切相关, 并且ROMA的水平随着病变恶性程度增加而持续增加^[21]。恶性肿瘤的级别越高, 细胞密度越高, 又进一步限制了水的扩散, 而Dslow值较ADCstand能够更准确地反映肿瘤内水分子纯扩散信息, 故与ROMA指数的相关性更高。

本研究未刻意排除交界性肿瘤、非卵巢上皮性恶性肿瘤和转移性肿瘤, 其目的是期望更好地模拟临床实际情况。但该研究仍有一定局限性, (1)本研究为回顾性分析, 样本量不够充足, 所选ROI的实性程度不同, 可能存在影响检测结果的微观囊变区; (2)本研究中低级别卵巢上皮癌的病例较少, 因此未进一步进行上皮性卵巢癌分级DWI定量参数比较。(3)卵巢IVIM-DWI扫描的合适b值设定仍然需要进一步优化。

综上所述, 基于IVIM-DWI多指数模型有助于卵巢肿瘤的良恶性鉴别, 其中参数Dslow、ADCstand及f诊断效能较高。参数ADCstand及Dslow卵巢恶性肿瘤ROMA指数具有相关性, 可作为卵巢良恶性肿瘤鉴别诊断的可靠影像学指标。

参考文献

[1] Torre LA, Trabert B, DeSantis CE, et al. Ovarian cancer statistics, 2018 [J]. *CA Cancer J Clin*, 2018, 68(4): 284–296.

[2] Duska LR, Kohn EC. The new classifications of ovarian, fallopian tube, and primary peritoneal cancer and their clinical implications. *Ann Oncol*, 2017, 28(suppl_8): viii18–viii12.

[3] Rizzo S, De Piano F, Buscarino V, et al. Pre-operative evaluation of epithelial ovarian cancer patients: Role of whole body diffusion weighted imaging MR and CT scans in the selection of patients suitable for primary debulking surgery. A single-centre study. *Eur J Radiol*, 2020, 123: 108786.

[4] Pi S, Cao R, Qiang JW, et al. Utility of DWI with quantitative ADC values in ovarian tumors: a meta-analysis of diagnostic test performance[J]. *Acta Radiol*, 2018, 59(11): 1386–1394.

[5] Le Bihan D, Breton E, Lallemand D, et al. Separation of diffusion and perfusion in intravoxel incoherent motion MR imaging[J]. *Radiology*, 1988, 168: 497–505.

[6] Seo N, Chung YE, Park YN, et al. Liver fibrosis: stretched exponential model outperforms mono-exponential and bi-exponential models of diffusion-weighted MRI. *Eur Radiol*, 2018, 28(7): 2812–2822.

[7] Cui R, Wang Y, Li Y, et al. Clinical value of ROMA index in diagnosis of ovarian cancer: meta-analysis[J]. *Cancer Manag Res*, 2019, 11: 2545–2551.

[8] 罗琰, 王沂峰, 陈高文. 卵巢恶性肿瘤风险算法在女性盆腔肿块良恶性鉴别诊断价值的荟萃分析[J]. *中华医学杂志*, 2019, 99(27): 2141–2144.

[9] Wilailak S, Chan KK, Chen CA, et al. Distinguishing benign from malignant pelvic mass utilizing an algorithm with HE4, menopausal status, and ultrasound findings[J]. *J Gynecol Oncol*, 2015, 26: 46–53.

[10] Iima M, Le Bihan D. Clinical intravoxel incoherent motion and diffusion MR imaging: Past, present, and future[J]. *Radiology*, 2016, 278: 13–32.

[11] Jiang J, Xiao Z, Tang Z, et al. Differentiating between benign and malignant sinonasal lesions using dynamic contrast-enhanced MRI and intravoxel incoherent motion[J]. *Eur J Radiol*, 2018, 98: 7–13.

[12] Garcia-Figueiras R, Padhani AR, Beer AJ, et al. Imaging of tumor angiogenesis for radiologists—Part 1: Biological and technical basis [J]. *Curr Probl Diagn Radiol*, 2015, 44: 407–424.

[13] 杨盼盼, 弓静, 王莉, 等. IVIM-DWI在女性附件病变中的应用价值研究[J]. *放射学实践*, 2019, 34(4): 450–455.

[14] Lin Y, Li J, Zhang Z, et al. Comparison of intravoxel incoherent motion diffusion-weighted MR imaging and arterial spin labeling MR imaging in gliomas[J]. *Biomed Res Int*, 2015, 2015: 234245.

[15] Andreou A, Koh DM, Collins DJ, et al. Measurement reproducibility of perfusion fraction and pseudodiffusion coefficient derived by intravoxel incoherent motion diffusion-weighted MR imaging in normal liver and metastases[J]. *European Radiology*, 2013, 23: 428–434.

[16] Cohen AD, Schieke MC, Hohenwarter MD, et al. The effect of low b-values on the intravoxel incoherent motion derived pseudodiffusion parameter in liver[J]. *Magnetic Resonance in Medicine*, 2015, 73: 306–311.

[17] Le Bihan D, Turner R. The capillary network: A link between IVIM and classical perfusion[J]. *Magn Reson Med*, 1992, 27: 171–178.

[18] Kwee TC, Galban CJ, Tsien C, et al. Comparison of apparent diffusion coefficients and distributed diffusion coefficients in high-grade gliomas[J]. *J Magn Reson Imaging*, 2010, 31: 531–537.

[19] Bennett KM, Schmainda KM, Bennett RT, et al. Characterization of continuously distributed cortical water diffusion rates with a stretched-exponential model[J]. *Magn Reson Med*, 2003, 50: 727–734.

[20] 陈志燕, 金力. 多囊卵巢综合征的高雄激素血症对生育的影响[J]. *中华妇产科杂志*, 2019, 54(6): 425–428.

[21] Ducheze V, Caillon H, Vaucel E, et al. Biomarkers and algorithms for diagnosis of ovarian cancer: CA125, HE4, RMI and ROMA, a review[J]. *J Ovarian Res*, 2019, 12(1): 28.

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